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Photoelectrochemical response of non-enzymatic glucose biosensing for graphene, carbon nanotubes and BiVO_4 nanocomposites

Syeda Ammara Shabbir^{1[,](http://orcid.org/0000-0003-3302-4634)*} (D, Ambreen Imran¹, Muhammad Gul Bahar Ashiq², Hamid Latif¹, Khalid Javed¹, and Mahroze Munam¹

¹ Department of Physics, Forman Christian College (A Chartered University), Lahore 54600, Pakistan 2 Department of Physics, College of Science, Imam Abdulrahman Bin Faisal University, P.O. Box 1982, Dammam 31441, Saudi Arabia

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ABSTRACT

Diabetes mellitus is a worldwide disease which affects the vital organs of human body. The approach executed in this project is to fabricate the nanocomposites of $BiVO₄$ by incorporating reduced graphene oxide (RGO) and carbon nanotubes (CNT) for photoelectrochemical non-enzymatic glucose detection. These different composites were prepared using electrochemical deposition method. X-ray Diffraction (XRD) and scanning electron microscope (SEM) analysis confirmed the structural details and surface morphology of these nanostructures, graphene sheet, BiVO₄ nanoparticles and of carbon nanotubes. UV–Vis analysis revealed the increasing trend in absorption of light and absorption edge, for $\frac{BiVO_4}{Ch}$, $\frac{CNT}{BiVO_4}$, $\frac{RGO}{BiVO_4}$ and $\frac{CNT}{RGO}{BiVO_4}$ electrodes, respectively. The photoelectrochemical response was measured through Linear Sweep voltammetry and increase in current density was observed from pure BiVO₄nanoparticles to $CNT/BiVO_4$ to $RGO/BiVO_4$ and to $CNT/RGO/BiVO₄$, due to incorporation of graphene and carbon nanotubes. The increasing glucose oxidation current was measured through cyclic voltammetry. It was observed that glucose oxidation peak was maximum for $CNT/RGO/BiVO₄$ electrode, as the incorporation of extremely conductive CNTs specifies several routes for the transportation of electrons and act as an impressive conductive binders to restrict the agglomeration of graphene nanosheets, thus enhancing the rate of electrons exchange. This study shows that CNT/RGO/BiVO4 electrode is the best photoelectrochemical electrode for non-enzymatic glucose detection for providing maximum sensitivity of 501.5 mA cm^{-2} mM⁻¹ and good stability with negligible current response from interference species.

Address correspondence to E-mail: ammaraanwar@fccollege.edu.pk

1 Introduction

Diabetes mellitus is an international public health issue, which is caused by the shortage of insulin and excess of glucose in the blood [[1\]](#page-9-0). This disease is the major cause of vital body organs failure. Therefore, regular glucose monitoring is integral to know whether medicines are working successfully [[2\]](#page-9-0). Blood glucose meters are usually based on enzymatic biosensors in which minor pin pricks are used to obtain blood for glucose detection. Enzymes are unstable as they lose their activity after a short period of time or they become denature with the variation in temperature. Enzymes are costly and depend upon ambient humidity levels. However, non-enzymatic biosensors are more stable and detects glucose through direct oxidation in the specimen. For regular glucose monitoring, non-enzymatic biosensors [\[3](#page-9-0), [4](#page-9-0)] are preferred. In order to make sure that sufficient insulin is given off at proper time, a regular monitoring system traces out correct quantity of glucose round the clock. Non-enzymatic biosensors also have some drawbacks. They are highly sensitive towards electroactive interfering species present in the blood. Metal electrodes can easily be poisoned by adsorbed intermediates present in the blood.

Due to these disadvantages, research trend is leading towards photoelectrochemical (PEC) biosensing for the detection of biomolecules [[5–](#page-9-0)[8\]](#page-10-0). Photoelectrochemical sensing is a low cost detection method and provides higher sensitivity. Efficiency of PEC sensor depends upon the photo catalytic ability of active material. It involves electron transfer reaction amongst photo active material, the electrode and the anode, when light falls on it [\[1](#page-9-0), [9](#page-10-0), [10](#page-10-0)]. PEC Sensors has the ability to combine the process of photo excitation and electrochemical detection, and this feature makes it more useful as electrochemical and optical sensors. Photoelectrochemical non-enzymatic biosensors comprising composites of GR-CdS quantum dots were successfully fabricated [\[11](#page-10-0), [12](#page-10-0)]. Some other nanomaterials such as $TiO₂-B$ nanorods graphene decorated with CdS, TiC-C nanoflower, $Cu₂$ O_2 –Ti O_2 , nanohybrid sheets of Bismuth oxychloride BiOCl–graphene have been utilized for non-enzymatic photoelectrochemical glucose biosensing [\[13–15](#page-10-0)].

Bismuth Vanadate has been given an extreme importance by the researchers, due to its less toxicity, high chemical stability, and small bandgap of about 2.4 eV. Researchers have also found that $BiVO₄$ shows excellent photocatalytic properties [\[16–19](#page-10-0)]. Properties of narrow bandgap facilitate the formation of photo induced charge carrier. The photogenerated holes of $\rm BiVO_4$ have a strong capability to oxidize organic matter that is attached to the surface, however, further research needs to explore in the area of application in non-enzymatic glucose sensors. Gopalan et al. [\[13](#page-10-0), [20\]](#page-10-0), successfully developed nonenzymatic photoelectrochemical glucose biosensor produced with the help of $BiVO₄$ electrode under visible light. However, due to insufficient transfer of charged particles and poorly adsorbed surface, the rate of recombination of electron–hole pair was high and thus it limited the photocatalytic properties of pure BiVO₄ [[21\]](#page-10-0). Therefore to enhance the photocatalytic properties of BiVO_4 , researchers explored different approaches like control of crystal Structure, combining with metal-oxides [[22\]](#page-10-0), non-metal doping [[23\]](#page-10-0) and nobel metal deposition [[24\]](#page-10-0). Carbon nanotubes being one dimensional material provide high conductivity with faster electron transfer rate. As graphene possesses distinctive nanostructure and exceptional properties, therefore graphene-based compounds have been the centre of attraction. Graphene-based compounds have been developed for different approaches like optical devices, sensors, catalysts. Graphene/TiO₂ nanocomposite was developed by Dai and his Co-workers, to show exceptional photocatalytic action in the degradation of Rhodamine B. Composite of Graphene/PtRu have been synthesized showing excellent electrocatalytic performance for methanol oxidation. The composite of BiVO4/rGO was developed to show the improved photocatalytic action in the degradation of RhB, by Xiong $[25]$ $[25]$. BiVO₄/rGO composite synthesized, by Yun Hau Na et al. as photocatalyst to exhibit improved photoelectrochemical effect in water splitting [\[26–28](#page-10-0)]. Therefore in this research project, the non-enzymatic photoelectrochemical glucose biosensing response of the electrodes based on composites of RGO, CNT and BiVO₄ nanoparticles, under visible light has been analyzed for the first time.

2 Experimentation

2.1 Materials

Bismuth Nitrate Pentahydrate $(Bi(NO₃)₃)$, Potassium Iodide (KI), Nitric Acid (HNO_{3),} Vanadyl Acetylacetonate (VO(acac)2), Dimethyl sulfoxide, Sodium Hydroxide (NaOH), COOH functionalized CNTs, sodium dodecyl sulphate (SDS), Hydrazine monohydrate, 1, 4-benzoquinone, Sulphuric acid (H_2SO_4) Hydrochloric acid (HCl), Sodium Nitrate (NaNO₃) Potassium Permanganate (KMnO₄)_, Hydrogen peroxide (H_2O_2) were all purchased from Sigma Aldrich.

2.2 Fabrication of $\rm BiVO_4$ electrode

For the fabrication of nanoporous electrode of $\rm BiVO_4$ on the flourine doped tin oxide glass, electrochemical deposition was used. In order to prepare the solution for platting, 40 mM $Bi(NO₃)₃·5H₂O$ was dissolved in 50 mL aqueous solution of 400 mM KI. Solution of opaque orange color was obtained. In order to calibrate its pH value to 1.75, few drops of dil. $HNO₃$ was added. The color of solution changed to transparent red–orange color. This solution was then dissolved with 0.23 M 1,4-benzoquinone in 20 mL of ethanol along with stirring for 10 min. Blackish solution of BiOI was obtained. The sample was prepared at electrodeposition time of 450 s and potential of $+$ 0.13 V. The BiOI electrode was thoroughly washed with DI water and then it was dried in oven for 15 min at 110 °C. Then 0.20 M of Vanadyl acetylacetonate was mixed in 5 mL dimethyl sulfoxide. Solution became emerald green in color. This mixture was drizzled uniformly on BiOI film. Then electrode was washed in DI water and ethanol and dried at room temperature.

2.3 Fabrication of CNT/BiVO₄ nanocomposite electrode

COOH (50 mg) functionalized CNTs were dissolved in Sodium Dodecyl Sulphate (0.075 g) and deionized water (50 mL). The solution was sonicated for 60 min and then centrifuged for 30 min at the rate of 8000 rpm. The resultant product was stable and homogeneous dispersal. This stable solution was then used for carbon nanotubes-based electrodes fabrication using spin coating. The solution was spin coated on FTO substrate at 3000 rpm for 80 s to

2.4 Fabrication of RGO/BiVO₄ nanocomposite electrode

Reduced Graphene oxide (RGO) was obtained by the modified Hummor's method. The reduced graphene oxide solution was spin coated on FTO substrate at 3000 rpm for 80 s with subsequent electrodeposition of BiVO₄ to fabricated RGO/BiVO₄ nanocomposite electrode.

2.5 Fabrication of CNT/RGO/BiVO₄ nanocomposite electrode

CNT is coated on FTO with sequential deposition of RGO and $BiVO₄$ to get CNT/RGO/BiVO₄ electrode.

2.6 Characterization of nanocomposite electrodes

Scanning electron microscope (SEM) was used to study the morphology of the $\rm BiVO_4$, $\rm CNT/BiVO_4$, RGO/BiVO4 and CNT/RGO/BiVO4 electrodes. The XRD spectrum was obtained from X-Ray diffractometer using CuKa radiation at 40 kV for identification of the required composite materials. The UV– Vis absorption spectra was obtained using the spectrophotometer.

2.7 Photoelectrochemical measurements

A 3-electrode system, with Pt as a counter electrode, saturated calomel electrode as reference electrode and the prepared $BiVO₄$ nanocomposites-based electrode as working electrodes, was setup for electrochemical measurements. For the Photoelectrochemical measurements 450 W Xe lamp with Am 1.5G filter and intensity of 100 mW cm^{-2} was used. The working electrodes geometric area of 2 cm^2 was kept constant. The photocatalytic activity of electrodes for glucose oxidation was examined using linear sweep voltammetry (LSV) and cyclic voltammetry (CV). Amperometric measurements were employed to measure the sensitivity, stability, reproducibility and interference of electrodes for glucose detection.

3 Results and discussion

The UV–Vis spectroscopy was conducted to observe the optical properties of the prepared samples of the Bismuth Vanadate composites. The Graphical analysis of UV–vis Spectroscopy of the four samples, $BiVO₄$, CNT/BiVO₄, RGO/BiVO₄, and CNT/RGO/ $BiVO₄$ is given in Fig. 1. The UV analysis shows increasing trend in the light absorption, respectively.

The absorption edge has also been calculated from Fig. 1. The BiVO₄ electrode shows absorption edge at 520 nm, $CNT/BiVO₄$ at 530 nm, $RGO/BiVO₄$ at 560 nm, and $CNT/RGO/BiVO₄$ at 600 nm. The introduction of CNTs and graphene in pure $BiVO₄$ nanoparticles has decreased the bandgap as a result of bond formation between them and thereby creating new energy states in the bandgap of $\rm BiVO_4$. This decrease in bandgap energy is responsible for increase in the absorption of light and absorption edge, respectively.

Bandgap energy is helpful in evaluating the photocatalytic properties. The relation of incident photon energy and absorbance is given by

 $Ahv = C(hv - E_g)ⁿ$

whereas absorption coefficient is represented by A, bandgap energy is represented by $E_{\rm g}$, h is the Planck's Constant, v shows the frequency of the incident light, C is the constant that is related to the mass of

Fig. 1 UV–vis spectroscopic analysis of BiVO4, CNT/BiVO4, RGO/BiVO4 and CNT/RGO/BiVO4, respectively

electrons and holes and the value of n depends on the type of transition ($n = 1/2$ for direct transition and $n = 2$ for indirect transition). The majority of the literature survey suggests that $BiVO₄$ follows direct transition. The optical bandgap energies were calculated using the Tauc relation, $(Ahv)^2$ versus h.

The calculated bandgap energies of pure $BiVO₄$ is 2.46 eV, of $CNT/BiVO₄$ is 2.3 eV, of RGO/BiVO₄ is 2.16 eV and of $CNT/RGO/BiVO₄$ is 1.6 eV as shown in Fig. [2.](#page-4-0) It is observed that incorporation of CNTs, RGO and CNT/RGO with $BiVO₄$ has decreased the bandgap energy value from 2.4 to 1.6 eV. Bandgap analysis is correlated with UV analysis. The lowest bandgap energy value of the composite CNT/RGO/ BiVO4 reveals increased absorption of light and increased absorption edge and thus creating more electron–hole pairs for photocatalysis in biosensing (Table [1\)](#page-4-0).

Scanning electron microscope (SEM) was used to determine the surface morphology of the prepared samples of BiVO₄, RGO/BiVO₄, CNT/BiVO₄, and $CNT/RGO/BiVO₄$ as shown in Figs. [3,](#page-5-0) [4,](#page-5-0) [5](#page-6-0) and [6](#page-7-0).

The SEM image of $BiVO₄$ in Fig. [3a](#page-5-0) confirms the spherical shape of $BiVO₄$ nanoparticles. This image reveals that the particle size ranges from 60 to 70 nm. The SEM image of $CNT/BiVO₄$ composite in Fig. [3b](#page-5-0) shows tubular structure of carbon nanotubes with attached BiVO₄ nanoparticles. The SEM image of $RGO/BiVO₄$ composite in Fig. [3c](#page-5-0) clearly shows that BiVO4 nanoparticles are uniformly embedded and well dispersed on the RGO sheets. This embedding of nanoparticles on RGO sheet plays important role in the increased transfer of electrons from $BiVO₄$ to RGO after the generation of photogenerated electrons exhibiting improved photocatalytic activity. The SEM image of the RGO/CNT/BiVO₄ composite in Fig. [3](#page-5-0)d shows graphene sheets wrapping the BiVO4 nanoparticles and the entangled CNTs on the surface of graphene sheets prohibits the agglomeration of graphene nano sheets thus enhancing the charge exchange effectively.

The crystal structure analysis of BiVO_4 , $\text{CNT}/$ $BiVO₄$, $RGO/BiVO₄$, and $CNT/RGO/BiVO₄$ composites are investigated through XRD analysis. The XRD patterns for all the samples are exhibited in Fig. [4](#page-5-0). The sharp diffraction peaks of $\rm BiVO_4$ are observed at 18°, 28°, 34°, 38°, 52°, 57°, 62° corresponding to (110), (121), (200), (002), (161), (251), and (132) diffraction planes respectively showing large crystallinity [[29\]](#page-10-0).

Fig. 2 a–d Tauc plots of BiVO₄, CNT/BiVO₄, RGO/BiVO₄ and CNT/RGO/BiVO₄

Table 1 Photoelectrochemical response regarding bandgap and absorption edge

| | Sample | | Bandgap (eV) Absorption edge (nm) |
|----|---------------------------|------|-----------------------------------|
| 1. | Pure $BiVO4$ | 2.46 | 520 |
| 2. | CNT/BiVO ₄ | 2.32 | 530 |
| 3. | rGO/BiVO ₄ | 2.16 | 560 |
| 4. | CNT/rGO/BiVO ₄ | 1.62 | 600 |

In the analysis of $CNT/BiVO₄$, an additional peak of plane (002), is observed at 26° , representing the graphitic peak due to the tubular structure of carbon atoms. For $RGO/BiVO₄$, a shorter peak (002) is observed at $2\theta \sim 26^\circ$ with decreased crystallinity which shows the successful reduction of GO into

RGO [[30,](#page-10-0) [31](#page-10-0)]. Lit. survey shows that graphite and RGO, both show a peak around 26° , however, the peak of graphite is sharp, whereas the peak of RGO is very small. In the $CNT/RGO/BiVO₄$ composite (002) is observed at 26° and this is not that sharp indicating the deposition of composite. Moreover, all overlapping peaks of $BiVO₄$ in $RGO/CNT/BVO$ may occur because the crystalline structure of $BiVO₄$ is larger than that of CNT and RGO.

The Linear sweep voltammetry (LSV) technique was used to analyse the photoelectrochemical response for $BiVO_4$, $RGO/BiVO_4$, $CNT/BiVO_4$ and RGO/CNT/BiVO4 nanocomposites electrodes. A solution of 0.1 M NaNO₃ was used to investigate the photocurrents generated with and without light

Fig. 3 SEM images for

Fig. 4 XRD patterns of BiVO₄, CNT/BiVO₄, RGO/BiVO₄ and CNT/RGO/BiVO4 composite

irradiation. The resulting current densities plot of the above samples are shown in Fig. [5](#page-6-0)a–e, respectively.

Figure [5a](#page-6-0) shows the current density in the absence of light for BiVO4 electrode. The current is approximately 0.25 mA cm^{-2} at all increasing applied potential values showing insignificant photocurrent response. BiVO₄ is a photoactive material so this graph is having no response in the absence of light. In the presence of visible light for BiVO4, the photo current increases as the applied potential increases as shown in Fig. [5b](#page-6-0) [\[22](#page-10-0), [31\]](#page-10-0).The maximum current density extends at 1.35038 mA cm^{-2} at 0.6 V versus SCE. In $CNT/BiVO₄$, upon light illumination, the current density attains the maximum value of

Fig. 5 LSV analysis for BiVO₄ in dark (a) in light for BiVO₄ (b), CNT/BiVO₄ (c), RGO/BiVO₄ (d) and CNT/RGO/BiVO₄ (e), respectively

Fig. 6 Cyclic voltametric curves of BiVO4, CNT/BiVO4, RGO/ BiVO4 and CNT/RGO/BiVO4 composite

1.3[5](#page-6-0)823 mA cm^{-2} at 0.6 V as shown in Fig. 5c. For RGO/BiVO4, the photocurrent reaches to the maximum value of 1.53261 mA cm^{-2} at 0.6 V as shown in Fig. [5d](#page-6-0). For CNT/RGO/BiVO₄, the maximum value of the current density is 1.85178 mA cm^{-2} at 0.6 V as shown in Fig. [5e](#page-6-0) upon light illumination. This analysis shows the increasing trend of current density in $BiVO₄$, $CNT/BiVO₄$, $RGO/BiVO₄$, and $CNT/RGO/A$ BiVO4, respectively. Upon illumination of light, the photogenerated holes in the valence band of BiVO4, with strong oxidizing ability, directly oxidizes the glucose adsorbed on the electrode surface. These electrons move through external circuit from anode to cathode and a current response is detected. When carbon nanotubes (CNT) were utilised as conducting support for $\rm BiVO_4$ nanoparticles, it increased the photoconversion efficiency because upon light irradiation of $\rm BiVO_4$, when electron hole pairs are generated, then there will be more charge transfer from $BiVO₄$ to the CNTs. The interaction between $BiVO₄$ and CNT played an important role for improving photoelectrochemical response as these one dimensional materials provide faster electron transport with increased electronic conductivity. In RGO/BiVO4, graphene sheets has provided large interfaces for collection and continuous pathways for photogenerated electron transfer to the electrode surface. It is difficult to have good distribution of BiVO4 nanoparticles on CNT in comparison to graphene sheet, because CNT agglomerate in bundle form. Therefore current density response of RGO/ BiVO₄ is higher than CNT/BiVO₄. In RGO/CNT/ $BiVO₄$, the composite of graphene and CNTs exhibits several benefits like the extremely conductive CNTs

specifies several routes for the transportation of electrons, which decreases the internal resistance. CNTs of 30 mm long intertwist with each other, and act as an impressive conductive binders which will hold the graphene nanosheets and the twisted CNTs on graphene nanosheets can behave such as to restrict the agglomeration of graphene nanosheets, thus enhancing the rate of electrons exchange. The increased value of the photocurrent for the composite of $CNT/RGO/BiVO₄$ confirms that this composite exhibits the tremendous photoelectrochemical response (Table 2).

3.1 Cyclic voltammetry

Cyclic voltammetry curves of all electrodes for the photoelectrochemical glucose oxidation were computed in 0.1 M solution of NaNO₃ under light irradiation and shown in Fig. 6. When glucose was added to the solution of $NaNO₃$, oxidation peaks at about $+$ 0.6 V, are observed as shown in Fig. 6.

The range of the potential was set from 1.0 to $-$ 0.9 V at the scan rate of 0.1 V s⁻¹. It is observed that anodic current peaks increases from $BiVO₄$, to $CNT/BiVO₄$, then to $RGO/BiVO₄$, and finally to $CNT/RGO/BiVO₄$. The photoelectrochemical response, observed in LSV, is also helping in the oxidation of glucose through cyclic voltammetry. Glucose is more efficiently oxidizing due to these parameters discussed in LSV analysis. Upon light irradiation electron hole pairs are generated in $BiVO₄$ and holes in the valence band helps for strong glucose oxidation at the electrodes. Electrons are transferred to electrode at a faster rate when CNT and RGO are employed in BiVO₄ electrode. As CNT and Graphene, both are conductive, CNTs are 1D and have faster electron transfer rate therefore significant increase in the anodic peak of $CNT/RGO/BiVO₄$ was observed. It shows that when CNT entangled on graphene sheets with $BiVO₄$ nanoparticles, it

Table 2 Photoelectrochemical response using LSV at 0.6 V potential

| | Sample | Current density (mA cm^{-2}) |
|----|---------------------------|---------------------------------|
| | BiVO ₄ | 1.35038 |
| 2. | CNT/BiVO ₄ | 1.35823 |
| 3. | RGO/BiVO ₄ | 1.53261 |
| | CNT/RGO/BiVO ₄ | 1.85178 |

restrains the agglomeration of graphene nanosheets, and as a result rate of electron exchange increases. Glucose oxidation peak was observed at 0.6 V and the corresponding current values are increasing from sample $BiVO₄$, $CNT/BiVO₄$, $RGO/BiVO₄$, $CNT/$ $RGO/BiVO₄$, respectively, shown in Table 3.

As shown in Fig. 7a, the amperometric photocurrent of the, $BiVO₄$, $CNT/BiVO₄$, $RGO/BiVO₄$ and CNT/RGO/BiVO4 electrodes have increased upon addition of glucose, and then rapidly reached a steady-state. The maximum photocurrent response during oxidation process of glucose has been detected for the CNT/RGO/BiVO4 electrode. These current responses suggest that the fabricated electrodes exhibit highly sensitive response towards the variable glucose concentration. Figure 7b shows the linear variation of glucose concentration with the current density. The glucose sensors have an excellent linear range. The correlation coefficient and sensitivity values were calculated from the graph. The slope equation for the linear curves evaluated the sensitivity values to be 501.5 mA cm^{-2} mM⁻¹, 431.5 mA cm^{-2} mM⁻¹ , 309.4 mA cm⁻² mM⁻¹, 121.3 mA cm⁻² mM⁻¹ for BiVO₄, CNT/BiVO₄, RGO/BiVO4 and CNT/RGO/BiVO4 electrodes, respectively. Thus CNT/RGO/BiVO₄ offered a visible light photoelectrochemical material with high sensitivity for non-enzymatic glucose sensing. This can be attributed to the high conductivity of graphene that successfully trapped the carbon nanotubes and nanoparticles in nanocomposite.

The high sensitivity of CNT/RGO/BiVO4 nanocomposite electrode reveals that it is highly efficient electrode for non-enzymatic glucose detection, therefore reproducibility, stability and interference test for this electrode was examined. Reproducibility of the electrode CNT/RGO/BiVO4 has been evaluated by measuring the amperometric generated current for five such similar electrodes. The relative standard deviation (RSD) of these five electrodes was evaluated to be 4.1%. Thus CNT/

Table 3 Current density for glucose detection response using cyclic voltammetry

| | Sample | Current density (mA cm^{-2}) |
|----|---------------------------|---------------------------------|
| 1. | BiVO ₄ | 30.12321 |
| 2. | CNT/BiVO ₄ | 61.23124 |
| 3. | RGO/BiVO ₄ | 73.05235 |
| 4. | CNT/RGO/BiVO ₄ | 81.29234 |

Fig. 7 a Photocurrent responses of the BiVO₄, $CNT/BiVO₄$, RGO/BiVO4 and CNT/RGO/BiVO4 nanocomposite electrodes with the successive addition of $10 \mu M$ glucose. **b** The amperometric current signal versus glucose concentration

RGO/BiVO4 electrode offers highly reproducible current for glucose detection. Inset of Fig. [8](#page-9-0) shows the stability analysis of CNT/RGO/BiVO₄ electrodes. This analysis was performed by measuring glucose detection response with 2 days interval. The magnitude of the current maintained about 90% after 23 days. This analysis examines the good stability of CNT/RGO/BiVO4 nanocomposite electrode.

Fig. 8 Interference response of CNT/RGO/BiVO₄ electrode. Inset: Stability evaluation of CNT/RGO/BiVO₄ electrode

In the interference analysis as shown in Fig. 8, current response was measured using intrusive species of uric acid, ascorbic acid and dopamine along with glucose. The comparison shows the major response of current signal due to glucose and negligible responses from the uric acid, ascorbic acid and dopamine. This analysis reveals that the CNT/RGO/ BiVO4 electrode is more sensitive for glucose in comparison to other species.

Thus CNT/RGO/BiVO4 electrode is an attractive material for non-enzymatic glucose detection with high sensitivity, reproducibility and stability.

4 Conclusion

A successful fabrication of nanocomposites-based electrodes of BiVO₄, CNT/BiVO₄, RGO/BiVO₄, $CNT/RGO/BiVO₄$, was accomplished as photoelectrochemical non-enzymatic biosensor, for the recognition of glucose, by the process of electrochemical deposition. The SEM and XRD analysis revealed the surface morphology and structural analysis of nanoparticles, nanotubes, and graphene sheets. The UV visible spectroscopic results showed increasing trend in light absorption with maximum absorption for $CNT/RGO/BiVO₄$ with a bandgap of 1.6 eV. This revealed the excellent photo absorption response of CNT/RGO/BiVO4 electrode due to decreased value of bandgap. This nanocomposite electrode with increased absorption spectrum excited greater number of electron hole pairs and encourages the effective charge carrier separation which decreases the rate of

recombination of electron hole pair, effectively. Under visible light irradiation, the photoelectrochemical behaviour was evaluated for all samples using Linear sweep voltammetry (LSV). The CNT/ RGO/BiVO4 electrode exhibited a greater photocurrent density of 1.85178 mA cm^{-2} (v/s SCE) in comparison to other fabricated electrodes, which is credited to highly conductive property of CNTs and RGO for providing several electron transfer pathways. Glucose detection response was measured through cyclic voltammetry. An increase in anodic peak current was observed with incorporation of CNT and RGO in BiVO4nanoparticles. The maximum anodic peak current and highest sensitivity value of 501.5 mA cm^{-2} mM⁻¹ for glucose oxidation was observed for CNT/RGO/BiVO4. The fabricated CNT/RGO/BiVO4 electrode, exhibited high stability and negligible current response from the interfering species.

Data availability

The datasets generated during and/or analysed during the current study are available from the corresponding author on reasonable request.

Declarations

Conflict of interest On behalf of all authors, the corresponding author states that there is no conflict of interest.

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